

The Fate of Porous Hydroxyapatite Granules Used in Facial Skeletal Augmentation

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Abstract Facial appearance is largely determined by the morphology of the underlying skeleton. Hydroxyapatite is one of several materials available to enhance projection of the facial skeleton. This study evaluated the long-term maintenance of augmented bony projection when porous hydroxyapatite granules are used on the facial skeleton. Ten female patients aged 28–58 years were studied following aesthetic augmentation of the facial skeleton at 24 sites using porous hydroxyapatite granules. Postoperative CT scans at 3 months served as the baseline measurement and compared with scans taken at 1 and 2 years, with the thickness of the hydroxyapatite measured in axial and coronal planes. Thickness of original bone plus overlay of hydroxyapatite, thickness of the overlying soft tissue, and the overall projection (bone plus soft tissue) were recorded. It was found that 99.7% of the hydroxyapatite was maintained at 2 years, with no statistical difference (*t* test) from the baseline measurement. The overall projection (bony and soft tissue) was maintained as there was no evidence of

native bone resorption or soft tissue atrophy. Radiographic results confirmed that the use of porous hydroxyapatite granules for enhancement of the facial skeleton is not only a predictable procedure, but maintains full bony projection at 2 years.

Keywords Hydroxyapatite · Facial augmentation · Facial skeleton · CT radiology

Facial appearance is largely determined by the morphology and relative prominence of areas of the underlying skeleton. With aging, areas of the facial skeleton undergo resorption contributing to laxity and descent of the soft tissue. Prominent “cheekbones” are considered youthful and prolong a younger appearance with aging [1–4] and a well-defined mandibular rim is fundamental to having a good and lasting neckline. Accordingly, surgical augmentation of the skeleton significantly enhances a person’s facial appearance and provides a more youthful look.

Augmentation of the facial skeleton has progressed since the early use of onlay silicone implants to treat malar asymmetries in the early 1960s [3]. The techniques developed initially for reconstructive surgery were employed for aesthetic indications in the early 1970s and included the use of both autogenous and alloplastic materials.

Autogenous bone grafts have been regarded as the preferred material for facial reconstruction. However, the disadvantages of donor site morbidity, limited moldability, and unpredictable postoperative resorption have limited their appeal for the aesthetic patient [5–8]. Accordingly, alloplastic implants derived from polymers and ceramics, usually in preformed shapes, have been favored in facial augmentation for aesthetic purposes [5, 8–14]. Preformed silicone and porous polyethylene (Medpor, Porex Corporation, Newman,

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GA) are currently the most used allografts. The recognized risks with these are minimal but include malposition, infection, thinning of the overlying soft tissues, and exposure [15, 16].

Hydroxyapatite is a biocompatible alloplast and a proven alternative for augmentation of the facial skeleton, having been used and studied for over two decades [10, 17–19]. Hydroxyapatite, a calcium phosphate compound $[\text{Ca}_{10}(\text{PO}_4)_6(\text{OH})_2]$, is the major mineral component of bone [9, 20–23] (Fig. 1). The porous, coral-derived type (Interpore 200, Interpore Orthopaedics, Inc., Irvine, CA) is formed by a hydrothermal exchange reaction of marine coral through the conversion of calcium carbonate coral to hydroxyapatite, which maintains the natural porous superstructure [17, 18]. Porous hydroxyapatite for augmentation is available in both granule and block form. The granular variant is associated with more predictable results and fewer complications [24]. In addition, the granular form requires considerably less operative exposure and soft tissue dissection.

A challenge associated with onlay implants is the prevention of postoperative movement and migration. An advantage of using hydroxyapatite is the inherent biological fixation, which means the graft is not prone to displace, extrude, or resorb which subsequently improves long-term results [5]. Previous studies have shown that the porous form (200 nm diameter) enables fibrovascular and, in some procedures, bony in-growth [25–27]. Hydroxyapatite is an alternative to bone grafts in orthognathic surgery and craniofacial reconstruction [28–32] and, in these applications, becomes subsequently incorporated into natural bone. Since the porous form of hydroxyapatite has been postulated to grow into bone in specific surgical procedures, although it is not osteoinductive [9, 19, 23, 27], it resists infection by creating a vascularized framework through the granules [16, 33–35]. Since it is biocompatible because it

has the same mineral composition as bone, hydroxyapatite is also readily incorporated within the subperiosteal layer without inducing a foreign-body reaction [17, 36–38]. The advantage of being highly malleable also allows intraoperative shaping for the desired result.

Hydroxyapatite is not used as widely as would be expected for augmentation of facial shape given its proven qualities of safety, versatility, and long-term use. A possible reason for this lack of popularity may be the absence of conclusive data regarding the long-term maintenance of the augmented volume. To evaluate the long-term fate of porous hydroxyapatite granules used in augmentation of the facial skeleton, a prospective radiologic study was performed over a 2-year follow-up period using thin-slice CT scans.

Materials and Methods

Over a 1-year period (2004–2005), 24 patients underwent augmentation of the facial skeleton for aesthetic enhancement using porous hydroxyapatite granules (Pro Osteon 200, Interpore Cross International, Irvine, CA). The procedures were performed by the senior surgeon (BCM). Ten patients agreed to be part of this prospective study. All were females between 28 and 58 years (mean = 42.9 years). Eight patients underwent additional procedures at the time of the facial skeletal augmentation, including blepharoplasty (6), facelift (5), browlift (1), rhinoplasty (1), and lipoinfiltration (2).

Preoperative planning for the location and quantity of hydroxyapatite to be used was determined by a trial volume injection using local anesthetic. The procedures were performed under general anesthesia with systemic antibiotic coverage (Cephalothin 1 g + Gentamicin 0.08 g). A precise subperiosteal pocket was made in the planned area of augmentation. A standard mixture of hydroxyapatite granules, fibrillar collagen (Spongostan Powder, Johnson & Johnson, Skipton, UK), and the patient's blood was prepared according to the technique recommended by Byrd [24]. An additional 20% was placed to allow for postoperative compaction associated with resolution of the degradable content of the injected mixture. The subperiosteal hydroxyapatite was then molded to obtain the desired contour. Several patients had augmentation at multiple sites.

With consent, ten patients completed three postoperative CT scans at 3 months, 1 year, and 2 years. All were performed by the same radiologist (ALM) using a GE Lightspeed 16 Multidetector-Row CT scanner (GE Healthcare, Milwaukee, WI). The patients were scanned supine with multislice acquisitions obtained in the axial plane through the relevant section of the face. The images were then reconstructed at 0.625 mm collimation with isotropic reconstructions—equivalent thickness to original axial

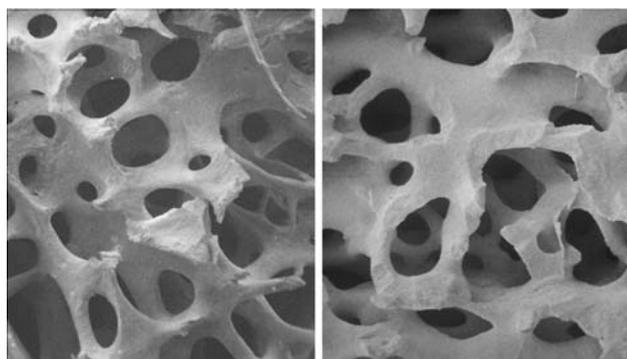


Fig. 1 Scanning electron micrographs of Pro Osteon 200 hydroxyapatite as used in augmentation of the facial skeleton (*left*) and the similar physical structure of human cancellous bone (*right*) (images courtesy of Interpore Cross International; reproduced with permission)

Fig. 2 Axial (*left*) and coronal (*right*) CT images showing hydroxyapatite overlying the body of the zygoma (shaded yellow on patient's right)

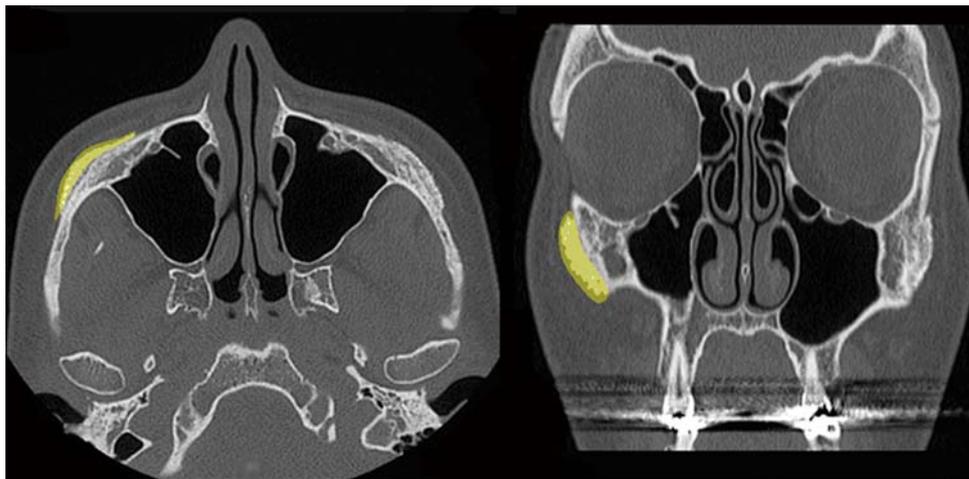
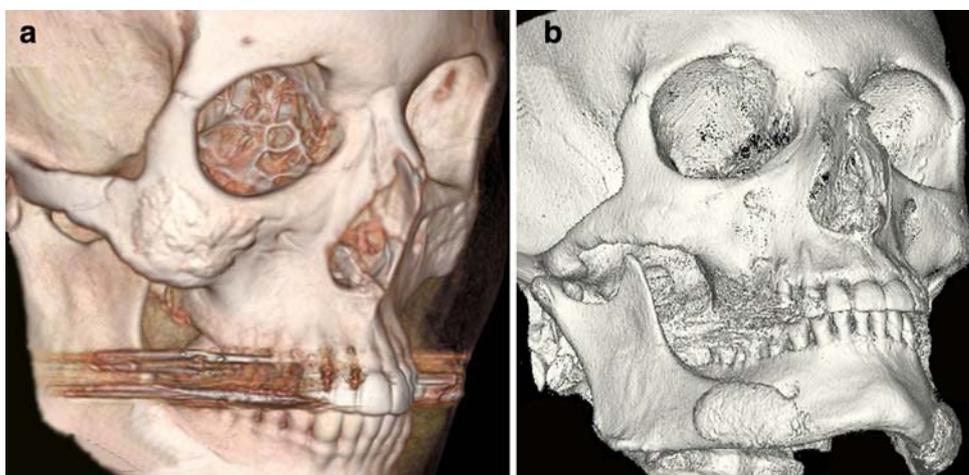


Fig. 3 3-D reconstructed CT images of the facial skeleton demonstrating the contour and thickness of hydroxyapatite placed over the zygomatic body (*left*) and prejowl region of mandibular body (*right*)



acquisitions in coronal, sagittal, and parasagittal planes (Fig. 2). Three-dimensional facial contour, bone contour, and volume-rendered reformatted images (Fig. 3) were completed on the GE AWA workstation. Measurements were taken in two planes (axial and coronal) where hydroxyapatite had been placed. Thickness of bone (original bone plus overlay of hydroxyapatite), thickness of the overlying soft tissue, and the overall projection (bone plus soft tissue) was recorded in millimeters. Linear measurements were more feasible than volumetric calculations and would similarly demonstrate the in situ behavior of the hydroxyapatite granules. The 3-month CT measurements served as the baseline and these results were compared with measurements obtained from the precise corresponding images on the 1- and 2-year CT scans.

The measurements acquired from the 1- and 2-year scans were each divided by the baseline measurement from the 3-month scan yielding a percentage of the baseline distance, i.e., 1-year measurement in mm/3-month measurement in mm and 2-year measurement in mm/3-month

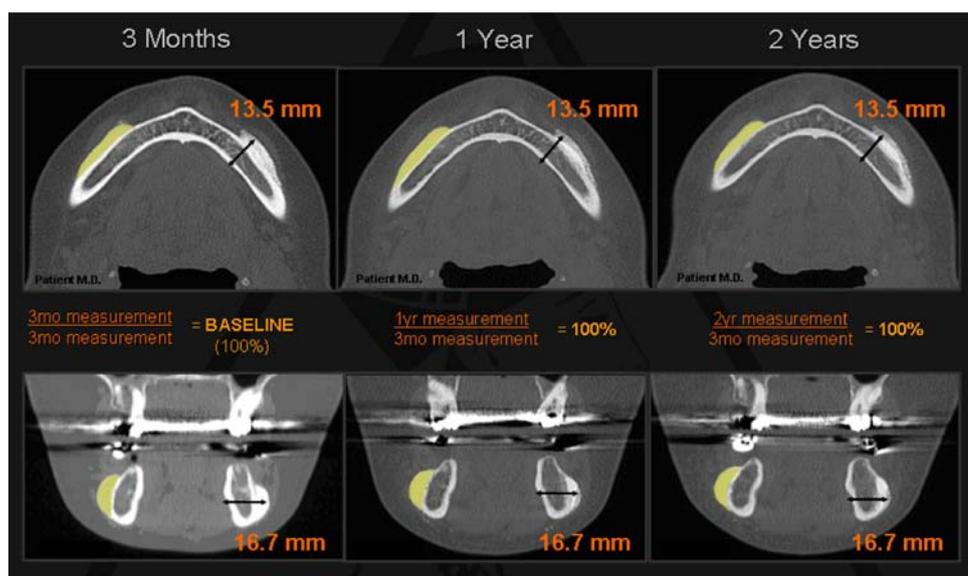
measurement in mm (Fig. 4). Statistical analysis was performed on the overall projection, bony thickness, and soft tissue thickness.

The patients' clinical charts were reviewed for age, location of augmentation, volume of hydroxyapatite used at each site, simultaneous procedures performed, complications, infection, local reaction, revision procedures, and the duration of clinical follow-up.

Results

The areas of skeletal augmentation included the prejowl region over the mandible (10), zygomaticomaxillary (10), and pyriform (4) regions. The average volume of hydroxyapatite granule mixture placed at each site was 1.6 ml (range = 0.4–3.5 ml). The radiological evaluation showed that 99.7% of the hydroxyapatite augmentation was maintained at 2 years when compared to the 3-month baseline measurements. The *t* test showed no statistical

Fig. 4 Axial (*top*) and corresponding coronal (*bottom*) CT images of the mandibular body showing the thickness of the hydroxyapatite maintained over a 2-year period (shaded yellow on patient's right)



difference. There was no radiographic evidence of soft tissue atrophy or native bone resorption on the 1- and 2-year scans. Overall projection (bony and soft tissue) was maintained at the 2-year follow-up.

Sequelae were limited to minor bruising, swelling, and moderate discomfort requiring a limited course of analgesia. No infections occurred during the 28 months of mean follow-up. One patient required a small revision procedure for aesthetic reasons. A small bulge of incorrectly placed granules over the mandibular rim was corrected by removal of localized excess granules and the associated fibrous tissue through the original incision.

Discussion

Underlying every attractive face is a skeleton that is proportional and well balanced. The unique form of the projection of the face determines the extent of a person's attractiveness [39]. The aesthetic outcome is ultimately determined by the facial soft tissue being well supported by a skeletal foundation [4]. Facial balance can be corrected or enhanced through augmentation of the zygomatic prominence, maxilla, mandible, nose, and supraorbital ridges [40] to achieve aesthetically pleasing proportions.

Beginning with Snyder's description of dermal grafts for treating malar facial agenesis in 1956 [41], many techniques and materials have since been used for augmentation of the facial skeleton. Osteotomies were introduced to enhance the morphology of the face [42], and subperiosteal autogenous bone grafts were utilized for unilateral corrective malarplasty [43, 44]. Alloplastic implants were soon developed in parallel to these techniques, with Hinderer using silicone [45] and Spadafora et al. using

polyethylene [46] for malar augmentation. Other alloplastic materials used have included ivory, metal, acrylic resins, and ceramics [16, 47]. Regardless of implant choice, all implanted materials should possess the basic attributes of being chemically inert, nontoxic, and incapable of inducing hypersensitivity or a foreign body reaction.

Combining hydroxyapatite granules with the patient's blood and additional collagen (Spongostan Powder) produces a material that provides the flexibility of tailoring the shape to the area of correction [24, 25, 27]. The mixture has a hemostatic effect and apparent resistance to infection [33]. There is little tendency for granule migration when the hydroxyapatite mixture is placed in a precise subperiosteal pocket [24, 25, 27]. Although the surgeon is required to custom-make the implant instead of using "off-the-shelf" alternatives, the need for specific fixation of the



Fig. 5 Intraoperative view immediately following placement of hydroxyapatite on the right maxilla and zygoma (2.8 ml granule mixture) with subperiosteal midcheek lift. Left side dissected but not yet augmented or lifted

Fig. 6 Preoperative (*left*) and 2-year postoperative (*right*) images and corresponding CT scans (*below*) following augmentation of the zygoma in a 25-year-old female demonstrating the improvement of soft tissue projection in the midface



implant, such as screws needed for porous polyethylene implants, is avoided. This is because of the biological integration of hydroxyapatite. Given the advantages of limited dissection, minimal morbidity, and minimal risk of complications, skeletal augmentation using hydroxyapatite widens the indications for its use so that patients who could benefit from a small-volume augmentation and are not candidates for traditional solid implants can reasonably benefit.

Compaction of the hydroxyapatite granules occurs during the first few weeks postsurgery and is completely stable by 6 months [48], with the postoperative reduction in projection averaging less than 10% [49, 50]. This is why baseline scans were obtained at 3 months to accommodate the anticipated settling and dimensional change.

Although this CT study had only a 2-year follow-up, the fact that the augmented volume is completely maintained suggests the result could be permanent. This is confirmed by other longer-term studies that report that hydroxyapatite maintains a permanent contour over 4 years, although those studies were clinical and less objective [6, 51, 52].

Augmentation of the facial skeleton is expected to become increasingly important as the expectations for aesthetic surgery results become more sophisticated. Now that there is no longer the uncertainty about the maintenance of the benefit when hydroxyapatite is used, it is reassuring that this approach to facial glamorization and rejuvenation is soundly based (Figs. 5, 6).

Conclusion

This study provides clear radiographic evidence that porous hydroxyapatite granules maintain bony and overall projection at 2 years when used for augmentation of the facial skeleton in the aesthetic patient. The completeness of the volume maintenance, although only over a 2-year follow-up in our study, suggests that the volume enhancement may be permanent.

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